

<u>Ultrasensitive Atomic Magnetometers</u>



Faculty

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Principles and Sensitivity of Atomic Magnetometry Application to Biomagnetism UW Portable Biomagnetometer

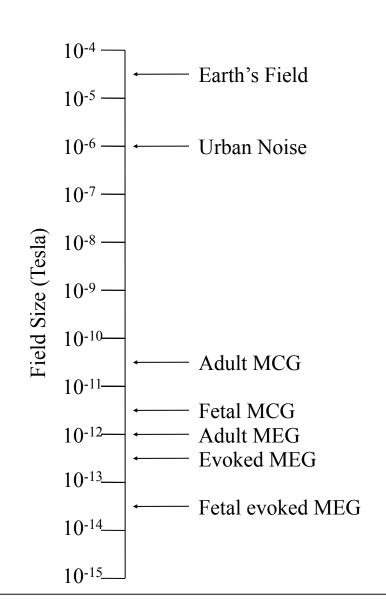








- Fetal MCG
- Puts requirements on magnetometer:
 - Sensitivity $\sim 10 \text{fT/Hz}^{1/2}$
 - Bandwidth ~ 100Hz

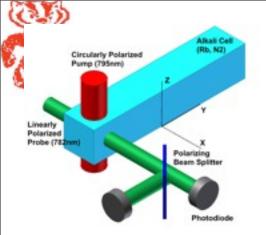




Highly Sensitive Magnetometers



| SQUID | Cryogenics Expensive | Can operate in large fields | Sensitivity ~1 fT/Hz ^{1/2} | High bandwidth (up to microwave frequencies) |
|------------------------|-------------------------|---------------------------------------|--|--|
| Atomic Magnetometer | Portable Inexpensive | Fully sensitive when in fields <10 nT | Sensitivity <1 fT/Hz ^{1/2} , shot noise limit <10aT/Hz ^{1/2} | Limited bandwidth |



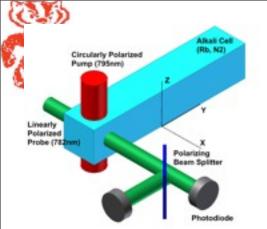


795nm

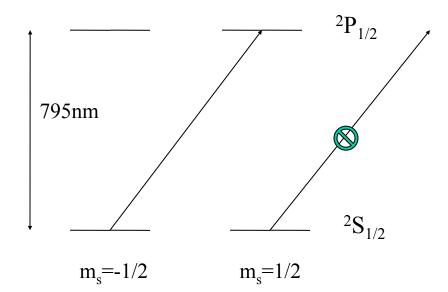
 $m_s = -1/2$

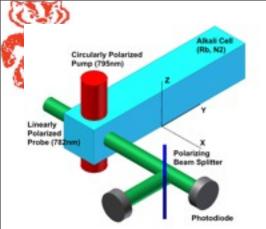
 $^{2}S_{1/2}$

 $m_{s} = 1/2$

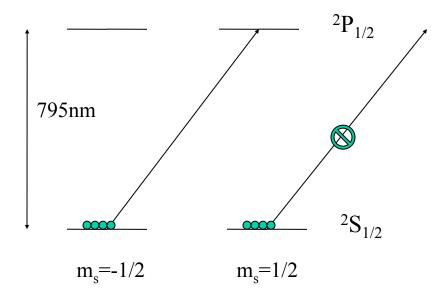


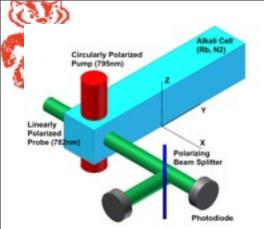




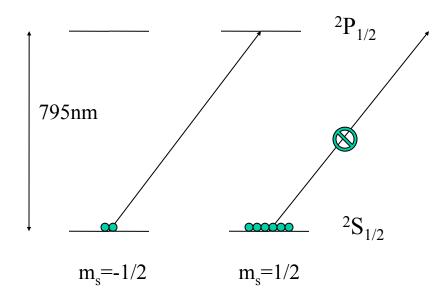


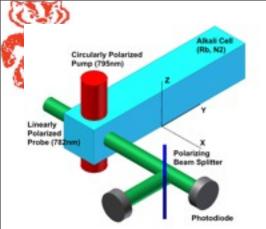




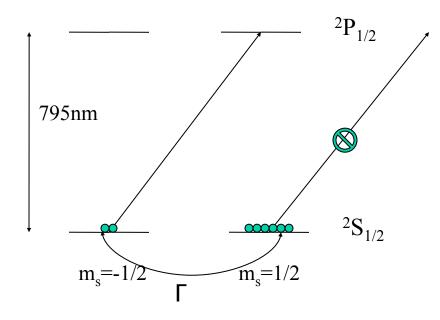


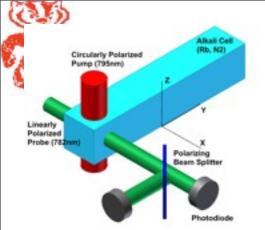




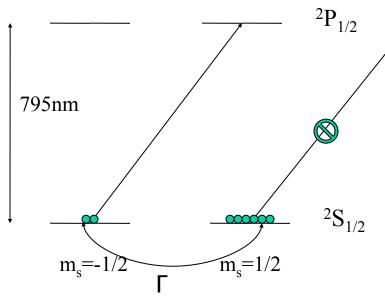












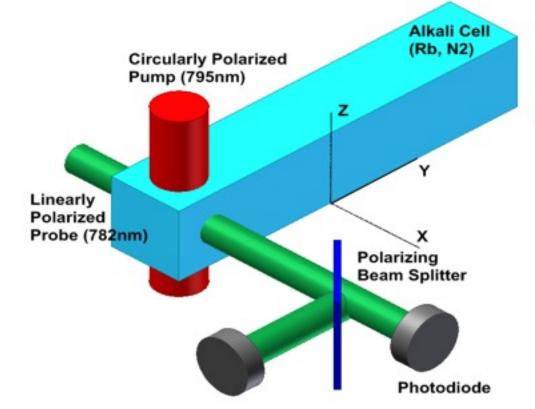
$$\frac{\mathsf{d}\left\langle \vec{F}\right\rangle}{\mathsf{d}t} = R\left(\frac{\vec{s}}{2} - \left\langle \vec{S}\right\rangle\right) - \Gamma\left\langle \vec{S}\right\rangle$$

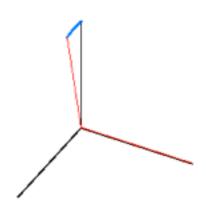






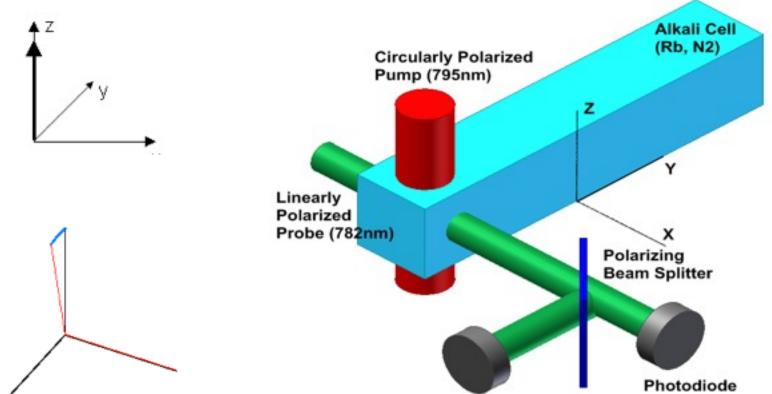






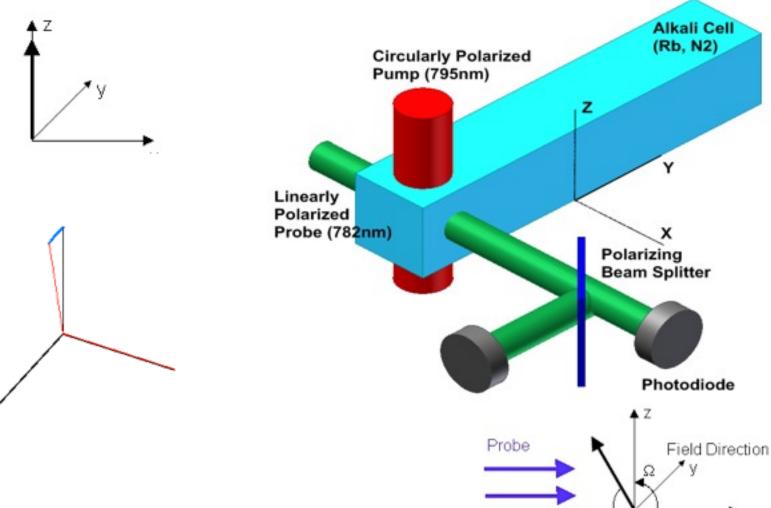








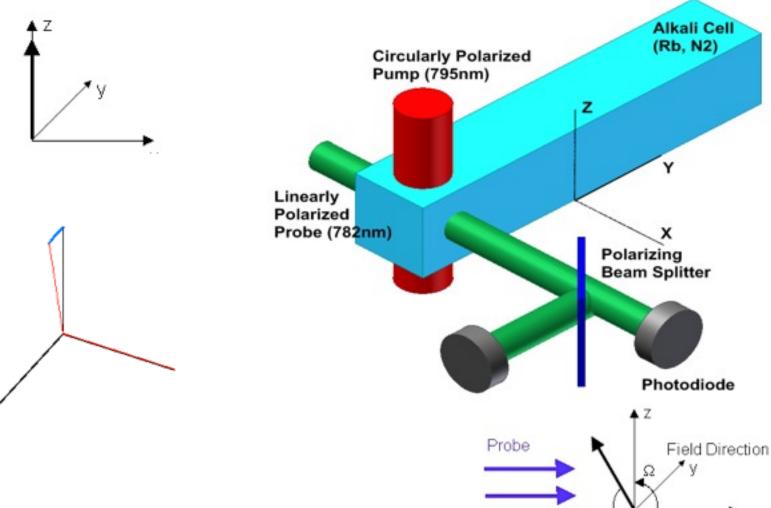




Faraday rotation of probe beam is $\sim \langle S_x \rangle$





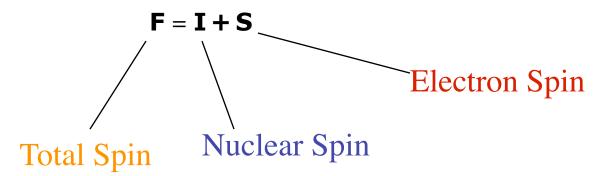


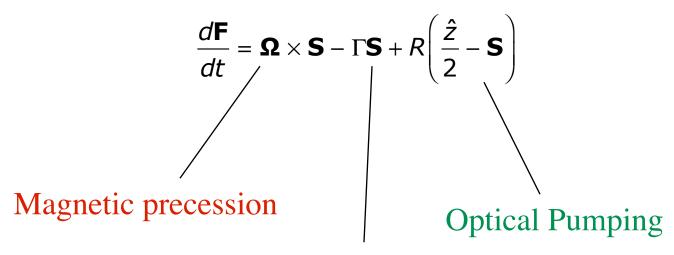
Faraday rotation of probe beam is $\sim \langle S_x \rangle$











Spin-Relaxation

DC Response:
$$S_x = S_z \frac{\Omega_y}{\Gamma + R}$$



Sensitivity



$$\delta B \approx \frac{\hbar}{g_s \mu_B} \sqrt{\frac{\Gamma}{nVT}}$$

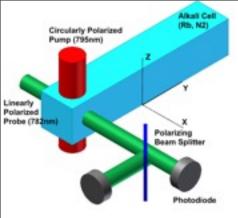
n = density; V = volume

T ≡ Measurement Time

Spin-Exchange Collisions: $\Gamma = n\sigma_{SE} \overline{V}$

Limits on traditional AM sensitivity:

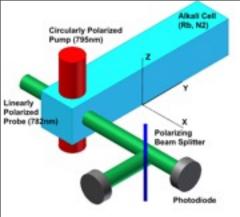
- •Traditional AM's had coherence times that were limited by Alkali-Alkali spin-exchange.
- •When density is turned up, the rate of these collisions increases, and $\Gamma / n \rightarrow \text{const.}$
- Shot noise limit ~10 fT/rt(Hz)



Spin-Exchange Collisions



Conserves **F**but redistributes
between **S** and **I**

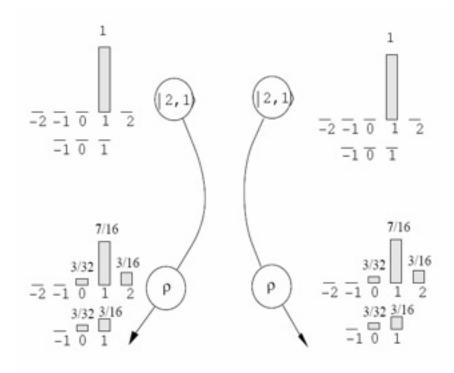


Spin-Exchange Collisions



Spin-Exchange Collisions

$$A(\uparrow)+B(\downarrow)\otimes A(\downarrow)+B(\uparrow)$$



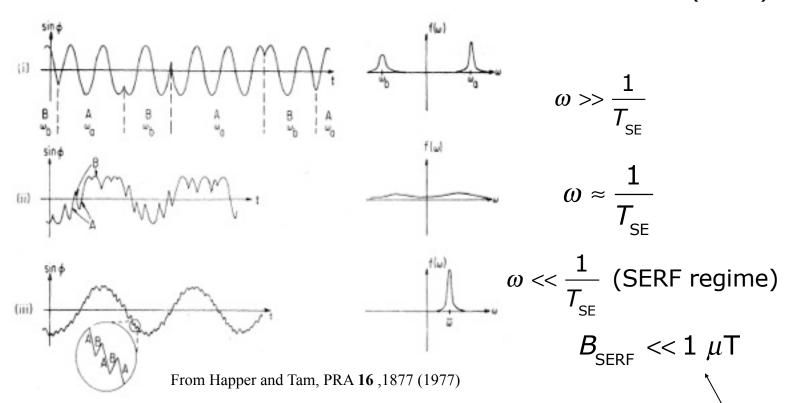
Conserves **F**but redistributes
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Spin-Exchange Relaxation Free (SERF) Regime



Larmor Frequency:
$$\vec{\omega}_{\vec{F}=\vec{I}\pm\frac{1}{2}} = \pm \frac{g_{J}\mu_{B}B}{(2I+1)\hbar}$$



• Operation in SERF regime allows the magnetometer sensitivity to depend on much weaker collisions with other atoms, hence several orders of magnitude greater sensitivity

Depends on alkali density

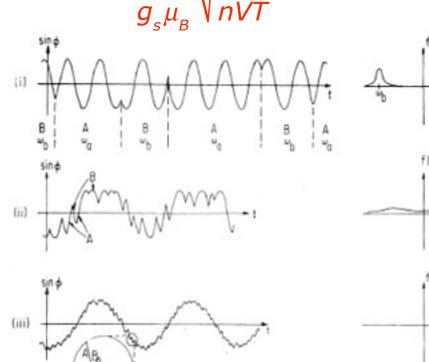


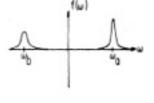
Spin-Exchange Relaxation Free (SERF) Regime



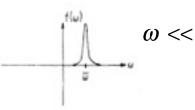
$$\delta B \approx \frac{\hbar}{g_s \mu_B} \sqrt{\frac{\Gamma}{nVT}}$$

Larmor Frequency:
$$\vec{\omega}_{\vec{F}=\vec{I}\pm\frac{1}{2}} = \pm \frac{g_{J}\mu_{B}B}{(2I+1)\hbar}$$









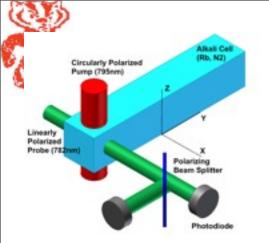
 $\omega \ll \frac{1}{T_{\rm SE}}$ (SERF regime)

$$B_{
m SERF} << 1~\mu {
m T}$$

• Operation in SERF regime allows the magnetometer sensitivity to depend on much weaker collisions with other atoms, hence several orders of magnitude greater sensitivity

From Happer and Tam, PRA 16, 1877 (1977)

Depends on alkali density



SERF Magnetometer

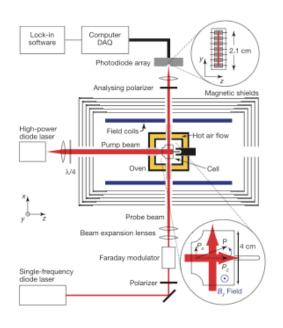


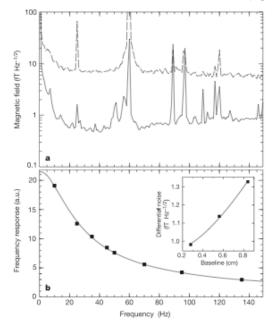
Rapid spin-exchange compared to the precession frequency leads to the spin-temperature distribution.

Links total spin to electron spin through "slowing down" factor. $\langle \mathbf{F} \rangle = q \langle \mathbf{\bar{S}} \rangle$ 4 < q < 6

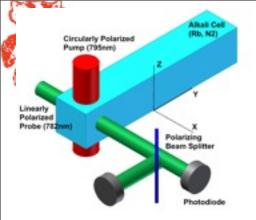
$$q\frac{d\mathbf{S}}{dt} = \mathbf{\Omega} \times \mathbf{S} - \mathbf{\Gamma}\mathbf{S} + R\left(\frac{\hat{z}}{2} - \mathbf{S}\right)$$

Spin-exchange does not contribute to Γ!





Kominis et. al. Nature 422, 596 (2003)



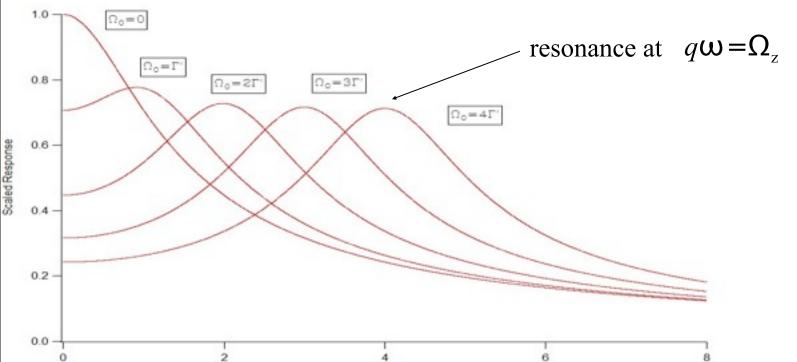
Frequency Response



If we apply a small oscillating field $\bar{\Omega}_1 = \Omega_1 \cos \omega t \hat{y}$

in the presence of a larger DC field
$$\vec{\Omega}_0 = \Omega_0 \hat{z}$$

$$\left| S_{1x} \right| = S_{z} \sqrt{\frac{\Omega_{1y}^{2} \left(\Gamma^{'2} + q \omega^{2} \right) + \Omega_{1x}^{2} \Omega_{0}}{\Gamma^{'4} + \left(\Omega_{0}^{2} - q^{2} \omega^{2} \right)^{2} + 2\Gamma^{'2} \left(\Omega_{0}^{2} + q^{2} \omega^{2} \right)}} \qquad \left| S_{1x} \right|_{\Omega_{0} \to 0} S_{z} \frac{\Omega_{1y}}{\sqrt{\Gamma^{'2} + q^{2} \omega^{2}}}$$



Thursday, September 10, 2009



DC Field Cancellation



SERF limit is about 1 μ T, but to get full sensitivity in our (DC) operation mode,

$$\omega_B < \frac{\Gamma_{SD}}{q(P)}$$
 gives $B < 30$ nT

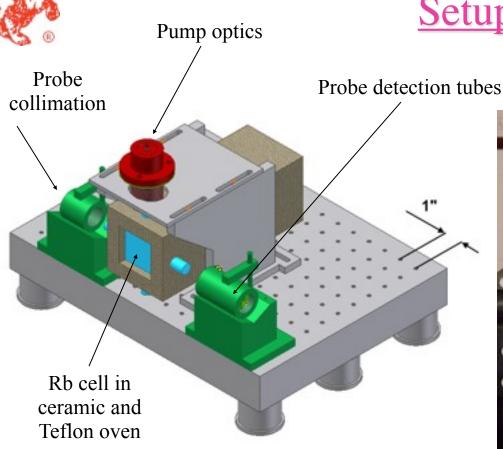
Residual field in our 4-layer shield is ~10s nT, so this requires further cancellation using triaxial Helmholtz coils. Automation of this process should be straightforward.

$$S_x = -S_z \frac{\Omega_y \Gamma' - \Omega_x \Omega_z}{\Omega^2 + \Gamma'^2}$$
 $\Gamma' = R + \Gamma_{SD}$
Shot-noise limit 20 aT/ $\sqrt{\text{Hz}}$ Allows easy residual field canceling



Setup







- Circularly polarized pump at 795nm
- Linearly polarized probe at ~780nm
- Cell heated to 180 C
- All lasers fiber coupled



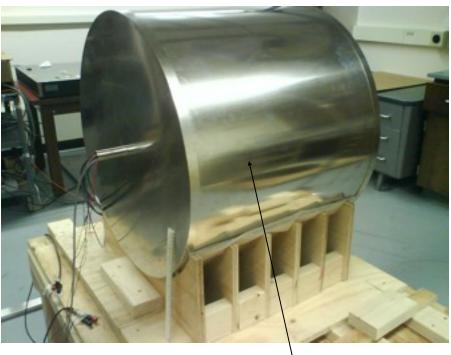
- Apparatus inside 4-layer mu-metal shield in lab
- Clinical use is in 3-layer shielded room



Some More Pictures







Tri-axial Helmholtz coils

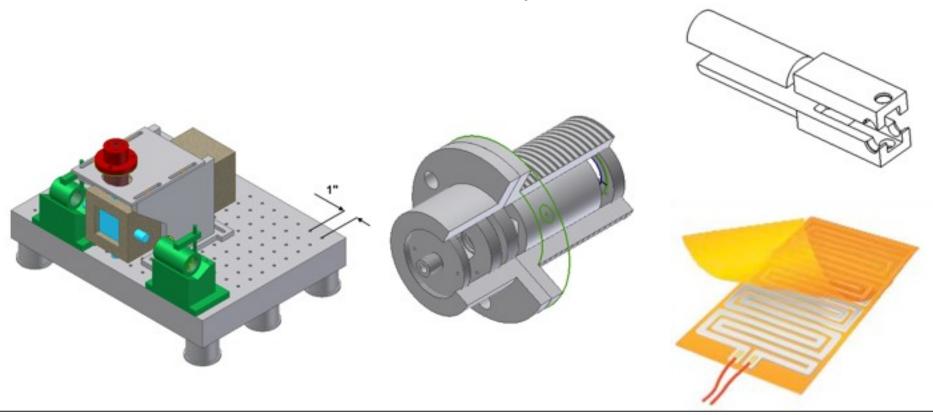
4-layer mu-metal shield



Technical Considerations



- Plastic, ceramic, and Teflon parts reduce Johnson noise
- Electric heating: dipole/quadrupole suppressed resistive film heater sandwich heats w/ small residual field (~100pT)
- Insulation allows subject to be 1cm away from Rb cell
- Simple 1-cm baseline gradiometer with pump tube
- Commercial 1 cm ×1 cm ×6 cm vapor cell



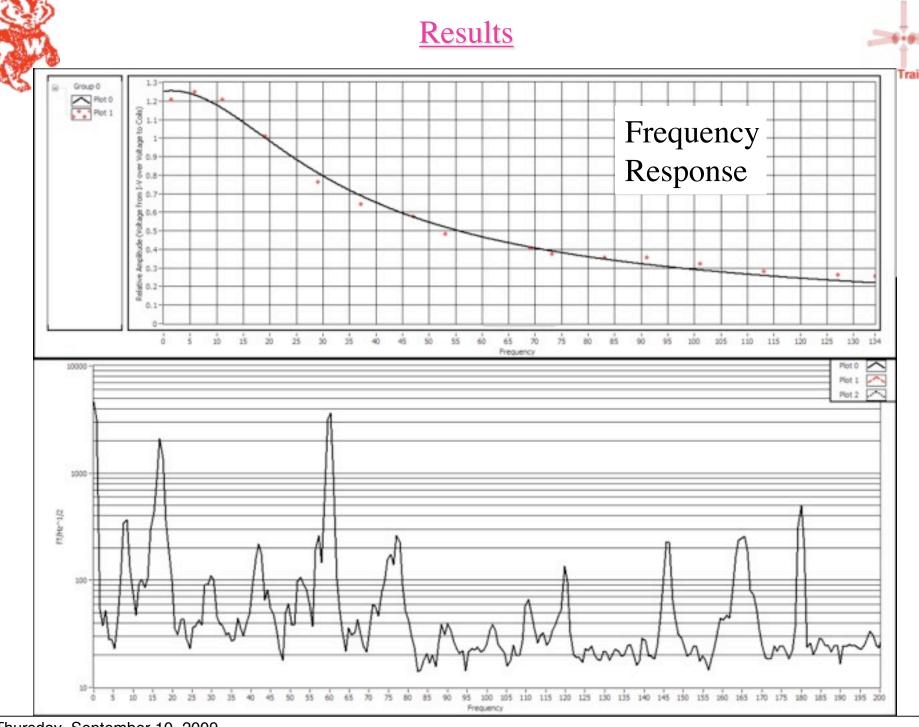


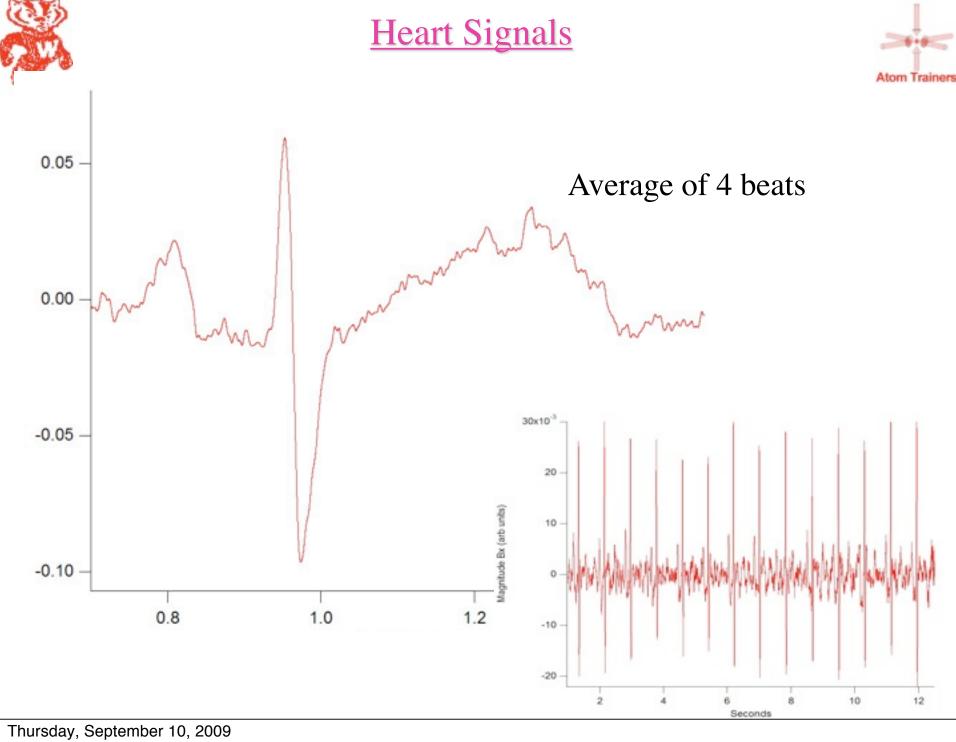


Portability



Bob Wyllie









Z-Mode

Z Li, R T Wakai, and T G Walker, Appl. Phys. Lett. 89, 134105 (2006)

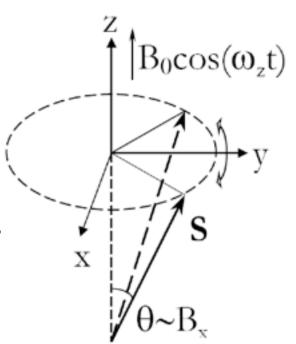
For best sensitivity, z-field Larmor frequency~parametric frequency, sets $B_z \approx 430 \text{nT}$

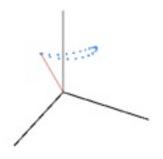
Allows us to run the magnetometer as a 2-component vector magnetometer

-Z1, Sx signal oscillates at ω_z for B_x

-Z2, Sx signal oscillates at $2\omega_z$ for B_y

Future: lock ω_{z} to Ω_{z} to measure changes in z-field

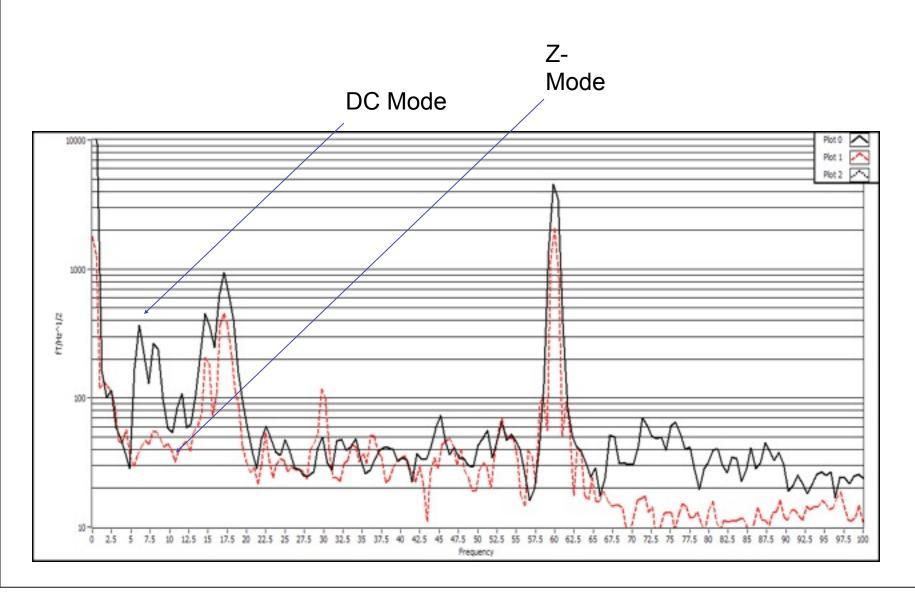








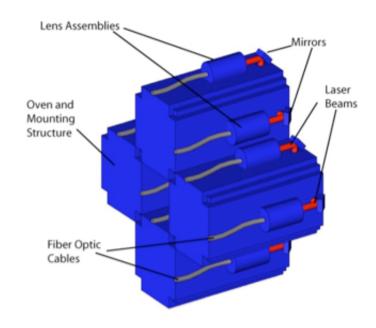
Technical Noise Reduction





Multichannel FMCG





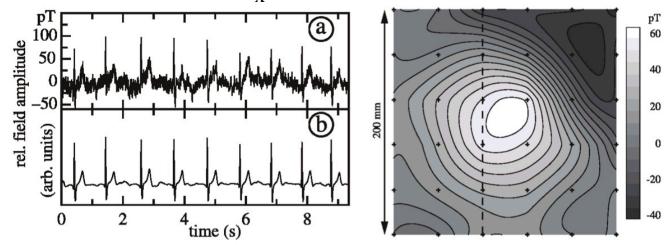
Should be easily miniaturized to a few cm/channel



Other AM MCG results



Shot-noise limited M_x non-SERF magnetometer



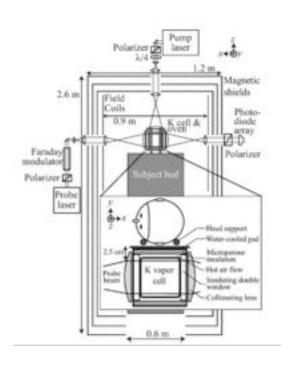
Bison et al., OPTICS EXPRESS 11, 904 (2003)

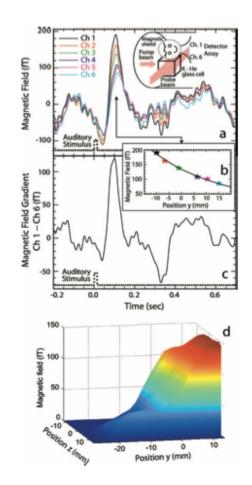
Poster 10-33 Measurement of Biomagnetic Fields in Small Animals by use of an Optical Pumping Atomic Magnetometer S. Taue et. al



Evoked MEG







XIA et al, APPLIED PHYSICS LETTERS 89, 211104

10-24 Development of a Wide-coverage Atomic Brain Magnetometer System (K. Kim, H. Xia, S. Lee, M.V. Romalis)



<u>Summary</u>



- Atomic magnetometers are performance-competitive with SQUIDs.
- Potentially substantially less expensive to build and operate
- Developed a portable, highly sensitive atomic magnetometer suited for fetal MCG measurements.
 - Sensitivity $\sim 40 \text{ fT/Hz}^{1/2}$
 - Bandwidth ~ 40 Hz
- Z-mode technical noise suppression and the ability to simultaneously detect two components of the magnetic field simultaneously.